Enhancing visual perceptual learning using transcranial electrical stimulation: Transcranial alternating current stimulation outperforms both transcranial direct current and random noise stimulation

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Diverse strategies can be employed to enhance skills, including visual perceptual learning (VPL transcranial electrical stimulation (tES). Combi and tES is a popular method that holds promis producing significant improvements in visual a within a short time frame. However, there is st	e visual .) and ning VPL e for cuity till a lack	(26 subjects each) to learn an orientation discrimin task with five daily training sessions. During trainin occipital region of each subject was stimulated by o type of tES—anodal transcranial direct current stimulation (tDCS), alternating current stimulation (tACS) at 10 Hz, high-frequency random noise	ation g, the one

of comprehensive evaluation regarding the effects of combining different types of tES and VPL on enhancing visual function, especially with a larger sample size. In the present study, we recruited four groups of subjects

stimulation (tRNS), and sham tACS—while the subject performed the training task. We found that, compared with the sham stimulation, both the high-frequency tRNS and the 10-Hz tACS facilitated VPL efficiently in

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terms of learning rate and performance improvement, but there was little modulatory effect in the anodal tDCS condition. Remarkably, the 10-Hz tACS condition exhibited superior modulatory effects compared with the tRNS condition, demonstrating the strongest modulation among the most commonly used tES types for further enhancing vision when combined with VPL. Our results suggest that alpha oscillations play a vital role in VPL. Our study provides a practical guide for vision rehabilitation.

Introduction

Our visual system is remarkably malleable (i.e., has visual plasticity) throughout the entire life span, for both mature and degenerative brains. It has been well documented that various methods can bring about visual plasticity, such as extensive training and non-invasive brain stimulation techniques (He, Yang, Zhao, & Fang, 2022). Regarding visual plasticity induced by extensive training (i.e., visual perceptual learning [VPL]), many advancements have been made in unveiling its characteristics, brain loci, and neural manifestations over the last three decades (He, Yang, & Zhao, 2022). More importantly, VPL has been widely applied in various elds (Lu, Lin, & Dosher, 2016), such as low-vision rehabilitation (Huang et al., 2022; Levi & Polat, 1996), remediation for dyslexia (Gori & Facoetti, 2014; Meng, Lin, Wang, Jiang, & Song, 2014), x-ray security screening (McCarley, Kramer, Wickens, Vidoni, & Boot, 2004), sports and military training (Hadlow, Panchuk, Mann, Portus, & Abernethy, 2018), and medical imaging education (Alexander, Waite, Macknik, & Martinez-Conde, 2020). At the same time, our visual plasticity can also be induced by transcranial electrical stimulation (tES)—a non-invasive neuromodulatory technique in which weak electrical elds are delivered through electrodes positioned on the scalp surface. The three most common types of tES techniques are categorized based on the current waveform: transcranial direct current stimulation (tDCS) (Nitsche & Paulus, 2000; Priori, Berardelli, Rona, Accornero, & Manfredi, 1998), transcranial alternating current stimulation (tACS) (Antal et al., 2008), and transcranial random noise stimulation (tRNS) (Terney, Chaieb, Moliadze, Antal, & Paulus, 2008). All of these three types of tES techniques have been found to be able to modify cortical excitability and modulate visual functions in both healthy and clinical populations (Bello et al., 2023), such as contrast sensitivity (Antal, Nitsche, & Paulus, 2001; Potok et al., 2023), visual acuity (Bocci et al., 2018; Reinhart, Xiao, McClenahan, & Woodman, 2016), motion direction discrimination (Battaglini et al., 2023; Ghin, Pavan, Contillo, & Mather, 2018), and peripheral target

identi cation in a crowded environment (Battaglini, Ghiani, Casco, & Ronconi, 2020; Chen, Zhu, He, & Fang, 2021), thus establishing causal links between brain activity and cognitive functions (Zhang, Zhang, Cai, Luo, & Fang, 2019).

Currently, there is an increasing focus on modulating VPL by tES, which is both theoretically signi cant and practically useful. Theoretically, through selective modulation of the brain during distinct phases of learning, mechanisms that support successful task acquisition and consolidation may be more fully characterized (He, Yang, & Fang, 2021; He, Yang, Gong, Bi, & Fang, 2022; He, Yang, & Zhao, 2022; Wu et al., 2023; Yang, He, & Fang, 2022). From the perspective of translational applications, attaining the greatest training bene ts e ect in the briefest time frame provides most bene t to subjects, whereas in a typical practical-oriented application case thousands of trials across multiple training sessions are usually required. Therefore, boosting VPL by tES is expected to accelerate learning and allow subjects to obtain greater bene ts (He, Yang, & Gong, 2022; Herpich et al., 2019).

Di erent types of tES have been adopted to modulate VPL (for a review, see He, Yang, & Zhao, 2022). With regard to the e ect of tDCS on modulating VPL, the results are mixed, and no consistent result has been found regardless of whether tDCS was administered before task execution (o ine mode) or during task execution (online mode). For example, when tDCS was applied during task execution, anodal tDCS was found to be e ective in boosting VPL in some studies (Frangou, Correia, & Kourtzi, 2018; Wu et al., 2023), but in other studies no obvious modulatory e ect was found (Fertonani, Pirulli, & Miniussi, 2011; Herpich et al., 2019; Larcombe, Kennard, O'Shea, & Bridge, 2018; Larcombe et al., 2018; Wu et al., 2022), and even a suppressive e ect was observed (Jia et al., 2022b). Studies using o ine tDCS in VPL tasks showed similarly con icting results (Pirulli, Fertonani, & Miniussi, 2013; Pirulli, Fertonani, & Miniussi, 2014; Wu et al., 2023). By contrast, the results of modulating VPL by tRNS are relatively consistent. Speci cally, high-frequency (100–640 Hz) tRNS boosts VPL e ectively in both healthy and clinical populations (Camilleri, Pavan, Ghin, Battaglini, & Campana, 2014; Campana, Camilleri, Pavan, Veronese, & Lo Giudice, 2014; Cappelletti, Pikkat, Upstill, Speekenbrink, & Walsh, 2015; Conto et al., 2021; Donkor et al., 2021). With regard to tACS, although the underlying neural mechanisms of action of tACS on the brain are relatively clear among tES techniques (Johnson et al., 2020; Krause, Vieira, Csorba, Pilly, & Pack, 2019; Zaehle, Rach, & Herrmann, 2010), only limited studies have been conducted to modulate VPL. Speci cally, when we previously stimulated subjects' visual cortical areas with tACS at di erent frequencies, we found that only occipital 10-Hz tACS was able to boost VPL,

and no such e ect was found for other stimulation frequencies (e.g., 6, 20, and 40 Hz) (He, Yang, & Gong, 2022). Similarly, in another study, occipital 3-Hz tACS was found to show little e ect on VPL (Zizlsperger, Kumrel & Haarmeier, 2016). Moreover, we also found that the modulatory e ect of 10-Hz tACS was absent when other cortical areas were stimulated (He, Yang, & Gong, 2022). Altogether, these studies demonstrate that tACS facilitates VPL in a frequencyand location-speci c manner. Despite advancements in VPL being observed

Despite advancements in VPL being observed blowing the application of diverse types of tES, a systematic evaluation of the modulatory e ects of tES in VPL is still lacking. Notably, studies on modulating VPL by tES usually employ a relatively small sample size design, raising the risk of sampling bias and miting the generalizability of those ndings (Minarik et al., 2016). We recruited four groups of subjects to earn an orientation discrimination task, and each moup received a speci c form of stimulation, including fram, tDCS, high-frequency tRNS, and 10-Hz tACS turing their training phase. Notably, there were 26 participants in each group, which provided su cient statistical power and representativeness to ensure the eliability and generalizability of our ndings.

Vlethods

Subjects

A total of 104 right-handed healthy adults with himal or correct-to-normal vision took part in the present study. Subjects were assigned to one of four onditions (26 subjects in each condition): anodal \mathbf{DCS} [11] females; mean age, 21.54 \pm 2.42 years), high-frequency tRNS (20 females; mean age, 21.77 \pm years), 10-Hz tACS (18 females; mean age, 21.15 58 years), and sham 10-Hz tACS (17 females; mean age, 22.04 ± 2.89 years). The sample sizes were determined based on our previous study (alpha level 0.05, power = 80%, two-tailed Cohen's d = 0.96(arg, & Gong, 2022). Speci cally, all data from study (He, Yang, & Gong, 2022) for the 10-Hz CS condition (n = 21) and the sham 10-Hz tACS ndition (n = 20) were included in the present study, and all other data were newly collected. We recruited e more subjects for the 10-Hz tACS condition and more subjects for the sham stimulation condition the present study to obtain more robust results. A eening questionnaire was administrated for each bjedt before starting the study. Subjects were excluded they met the following criteria: (1) age older than years or younger than 18 years, (2) a history of neural surgery or epileptic seizures or any psychiatric heurological disorders, (3) sleep disorders or a

total sleep time less than 7 hours per night over the last 2 weeks, or (4) during the ovulation phase of the menstrual cycle or pregnancy (He et al., 2019; He, Yang, & Gong, 2022). All experimental protocols and procedures were approved by the Ethics Committee of the School of Psychological and Cognitive Sciences at Peking University. Before participation, informed written consent was obtained from each subject.

Apparatus and stimulation protocol

MATLAB R2015a (MathWorks, Natick, MA) and Psychtoolbox-3 extensions (Brainard, 1997) were used to generate and control visual stimuli, which were presented on a liquid crystal display (LCD) monitor (Display + LCD Monitor; Cambridge ResearchSystems, Rochester, UK) with a gray background (mean luminance = 30 cd/m^2 , width = 70 cm, spatial resolution = 1920×1080 pixels, refresh rate = 120 Hz). The only source of light in the room was the monitor. The head of each subject was xed on a chin and head rest at a viewing distance of 70 cm. To ensure that the subject's eye position was stable within 1° from the xation point when visual stimuli were presented, the EyeLink 1000 Plus eye-tracking system (SR Research Ltd., Ottawa, ON, Canada) was used to monitor subjects' eye movements throughout the entire experiment.

The high-frequency (100–640 Hz) tRNS was delivered by a battery-powered current stimulator (DC-Stimulator Plus; neuroConn GmbH, Ilmenau, Germany), and the current in other forms was delivered using the DC-Stimulator MC (neuroConn) through a pair of rubber electrodes that were 5×7 cm². The ep e tric(. -0.00)] TJ /4n(e)0.) e684(hen)-S8.2(neur)33.-



Figure 1. Stimuli, experimental design, and electrical stimulation protocol. (A) Schematic description of a 2AFC trial in a QUEST staircase for measuring orientation discrimination thresholds. Subjects were instructed to make a judgment of the orientation in the second interval relative to that in the first interval (clockwise or counterclockwise) while gazing at the central fixation point. No feedback was provided after each trial. (B) Experimental protocol. Subjects underwent a pretraining test, five daily training sessions, and a post-training test. The pretraining test (Pre) and post-training test (Post) took place on the days before and immediately after training, respectively. The tES was concurrently administrated during each training session. (C) Electrical stimulation protocol and montage. tES with different current waveforms (tDCS, tRNS, and tACS) was applied concurrently during each training session. Stimulation electrodes were positioned over the occipital cortex (O2) and the vertex (Cz). The electrode positions were defined by the international 10–20 EEG system. The red square and blue square denote the anodal electrode and cathodal electrode, respectively. These head models were generated by FaceGen Modeller 3.4.

of the pixels in these patches were replaced with random noise) were presented in the lower left quadrant of the visual eld, 5° from the xation point. In each trial, a small xation point was presented rst for 500 ms. followed by two Gabor patches with orientations of 26° and 26° + θ , which appeared 100 ms each in a random order with a 500-ms blank interval (Figure 1A). A two-alternative forced-choice (2AFC) method was used in the task, and subjects were instructed to judge the orientation change of the second Gabor patch relative to the rst one (counterclockwise or clockwise) by pressing keys. Subjects' orientation discrimination thresholds at 75% accuracy were estimated using a QUEST staircase procedure, such that the θ varied trial by trial (Watson & Pelli, 1983). Subjects rested after each staircase. No feedback was provided in all test and training sessions.

Design

A single-blind, sham-controlled, between-subjects design was adopted to explore the modulatory e ect of di erent types of tES on orientation discrimination learning. Subjects were trained on the orientation discrimination task for ve consecutive days. Before and after the ve daily training sessions, test sessions were conducted: pretraining (Pre) and post-training (Post) (Figure 1B). Each test session and each training session consisted of six and nine QUEST staircases of 50 trials, respectively.

The hemisphere contralateral to the visual eld where the visual stimuli were presented was stimulated. Two electrodes were placed over each subject's visual cortex and vertex (i.e., O2 and Cz in the international 10–20 EEG system, respectively) (Figure 1C). Electrical

Statistical analysis

The threshold for each session was estimated by calculating the geometric mean of thresholds from all QUEST staircases in that session. The performance change after training was quanti ed by calculating the percent improvement as [(pretraining threshold – post-training threshold)/pretraining threshold $\times 100\%$. All estimated thresholds were then normalized: The estimated threshold for each session was divided by the estimated threshold at Pre and then multiplied by 100%. In order to describe the process of threshold change during the learning course, we tted the learning curves of normalized orientation discrimination thresholds across all sessions using a power function:

 $\log_{10} \left(Th\left(t \right) \right) = \rho \times \log_{10}(t)$

In this function, *Th* represents the predicted normalized threshold, t is the number of training sessions, and ρ is the learning rate (Yang et al., 2020). The threshold declines with training, such that the value of ρ should be negative, and a smaller value indicates a faster learning speed. To minimize the sum of squared di erences between model predictions and observed values, a nonlinear, least-square method was implemented in MATLAB.

A mixed-design analysis of variance (ANOVA) using Condition as a between-subjects factor (tDCS, tRNS, tACS, and sham) was used to analyze the orientation discrimination thresholds. Raw thresholds at Pre, learning rates, and percent improvements were analyzed by ANOVA using Condition as a between-subjects factor. We used the Benjamini-Hochberg method to control the false discovery rate for multiple comparisons. Partial eta squared (η_p^2) and Cohen's *d* were calculated to measure the e ect size for ANOVAs and t-tests. Statistical analyses were conducted using R (R Foundation for Statistical Computing, Vienna, Austria) (R Core Team, 2023).

Results

Training improved task performance substantially

First, a one-way ANOVA with Condition (tDCS, tRNS, tACS, and sham) as a between-subjects factor on the thresholds at Pre was conducted to examine

the baseline variance among all enrolled conditions. The statistical results showed that the main e ect of *Condition* was not signi cant, F(3, 100) = 0.37, p = 0.79, $\eta_p^2 = 0.01$, demonstrating that subjects had comparable baseline performance across all stimulation conditions (Figure 2A). Next, to assess the learning e ect on the trained task, we employed a mixed-design ANOVA that incorporated Session (Pre and Post) as a within-subjects factor, Condition as a between-subjects factor, and the subjects' orientation discrimination thresholds as the dependent variable. The statistical results showed that the main e ect of Session, F(1, 100) = 207.89, p < 0.001, $\eta_p^2 = 0.68$, and the interaction between *Session* and *Condition*, F(3, 100) = 3.29, p = 0.02, $\eta_p^2 = 0.09$, were signi cant, but the main e ect of *Condition*, F(3, 100) =0.95, p = 0.42, was not signi cant, demonstrating that the subjects' performance improved after training and the performance improvement was di erent across all stimulation conditions. Further analyses showed that the thresholds at Post were lower than those at Pre for all stimulation conditions: for sham, t(25) = 4.33, p_{adi} < 0.001, Cohen's d = 0.85; for tDCS, t(25) = 6.77, p_{adi} < 0.001, Cohen's d = 1.33; for tRNS, t(25) = 10.21, p_{adi} < 0.001, Cohen's d = 2.00; for tACS, t(25) = 9.01, p_{adi} < 0.001, Cohen's d = 1.77 (Figure 2B). Importantly, no feedback was provided during the training course, suggesting that subjects acquired the improved ability to discriminate the trained stimuli in an unsupervised learning manner (Frank et al., 2020; Tsodyks & Gilbert, 2004).

Learning rate was modulated by tES



Figure 2. Main results. (A) Thresholds at Pre. (B) Normalized learning curves. Dots represent averaged thresholds across subjects at different test and training sessions, and lines represent fitted learning curves using a power function. Note that the *y*-axis is displayed on a logarithmic scale. (C) Learning rate for each condition; a smaller value indicates a faster learning speed. (D) Percentage of improvement in orientation discrimination performance. * $p \le 0.05$; ** $p \le 0.01$; *** $p \le 0.001$. Error bars denote 1 *SEM* across subjects.

rate in the tACS condition was higher than that in the tRNS condition, t(50) = 2.27, $p_{adj} = 0.04$, Cohen's d = 0.63. In short, the application of 10-Hz tACS during training yielded the most rapid acceleration of the orientation discrimination learning.

Performance improvement was modulated by tES

The space for improvement in learning is of great concern to both basic and clinical researchers. Here, we examined percent improvement di erences among the di erent stimulation conditions. Percent improvement among the stimulation conditions was signi cant, as revealed by a one-way ANOVA, F(3, 100) = 9.69, p < 0.001, $\eta_p^2 = 0.23$ (Figure 2D). Further analyses showed that the percent improvement in the 10-Hz tACS condition was signi cantly higher than those in all other stimulation conditions: for tACS versus sham, t(50) = 4.85, $p_{adj} < 0.001$, Cohen's d = 1.35; for tACS versus

tDCS, t(50) = 3.08, $p_{adj} = 0.008$, Cohen's d = 0.85; for tACS versus tRNS, t(50) = 2.33, $p_{adj} = 0.04$, Cohen's d = 0.65. Notably, the performance improvement in the tRNS condition was signi cantly higher than that in the sham condition, t(50) = 3.55, $p_{adj} = 0.003$, Cohen's d = 0.98. All other di erences among the stimulation conditions were not signi cant: for tDCS versus sham, t(50) = 1.74, $p_{adj} = 0.11$, Cohen's d = 0.48; for tDCS versus tRNS, t(50) = 1.60, $p_{adj} = 0.12$, Cohen's d = 0.44. In short, after training with concurrent occipital 10-Hz tACS, subjects exhibited the most pronounced improvement in their performance on the trained orientation discrimination task.

In summary, subjects' task performance improved with training from comparable initial performance levels. The modulatory e ects of tES on VPL were strongly dependent on the stimulation type. Speci cally, anodal tDCS applied during execution of the orientation discrimination task had little e ect on modulating the acquisition of learning to discriminate the stimuli. By contrast, both high-frequency tRNS and 10-Hz tACS were capable of facilitating orientation discrimination learning, in terms of both learning rate and overall performance improvement achieved. Finally, occipital 10-Hz tACS showed the best modulatory e ects.

Discussion

In the present study, we evaluated the e ect of several of the most common types of tES techniques (i.e., tDCS, tRNS, and 10-Hz tACS) on the further enhancement of vision by modulating VPL. Our results revealed distinct modulatory e ects of tES with di erent current forms when applied during learning on the orientation discrimination task. Speci cally, compared with the sham stimulation, anodal tDCS showed little e ect on modulating VPL, but both high-frequency tRNS and 10-Hz tACS were e ective in boosting VPL. Additionally, 10-Hz tACS exhibited a superior modulatory e ect compared to the other current stimulation forms. To the best of our knowledge, the current study is the rst to systematically evaluate the e ects of various types of tES techniques on modulating VPL. Importantly, compared with previous studies investigating the modulatory e ects of tES on VPL, the present study has the largest sample size (\sim 30 subjects per condition), thus ensuring su cient statistical power for between-condition comparisons. In short, our ndings will provide guidance for translational applications of combining VPL and tES, as well as insights into the neural mechanisms of VPL.

We found that anodal tDCS applied concurrently with training had no e ect on modulating VPL, which is consistent with previous studies in short-term orientation discrimination learning (Fertonani et al., **2011**) or in multi-session learning on motion direction discrimination (Fertonani, Pirulli, Bollini, Miniussi, & Bortoletto, 2019; Herpich et al., 2019; Larcombe & Kennard, 2018; Larcombe & Kulyomina, 2018; Wu et al., 2022). However, our results are not consistent with some studies in which anodal tDCS was e ective in facilitating VPL (Olma et al., 2013; Sczesny-Kaiser et al., 2016; Van Meel, Daniels, de Beeck, & Baeck, 2016; Wu et al., 2023), or even impairing VPL with a short training session (Grasso, Tonolli, Bortoletto, & Miniussi, 2021; Grasso, Tonolli, & Miniussi, 2020; Jia et al., 2022a; Learmonth, Thut, Benwell, & Harvey, 2015). The discrepancies among these studies mentioned above can be caused by many factors, such as training tasks, training regimes, and stimulation settings. Of note, the small sample sizes adopted in previous studies may have biased the results (Minarik et al., 2016). Here, using a relatively large sample size design, we found that applying anodal tDCS concurrently during training had a negligible e ect on enhancing VPL. The null e ect

of anodal tDCS on modulating VPL during training might be caused by the timing of the stimulation applied. Previous studies have found that anodal tDCS applied prior to task execution (i.e., the o ine mode) was e ective in boosting VPL (Pirulli et al., 2013), but no such modulatory e ect was found when anodal tDCS was administrated during performance of the orientation discrimination task (i.e., the online mode) (Pirulli et al., 2013), just like the ndings in the present study.

We found that high-frequency tRNS was e ective in boosting VPL, which is consistent with previous studies (Camilleri et al., 2014; Camilleri, Pavan, & Campana, 2016; Contemori, Trotter, Cottereau, & Maniglia, 2019; Conto et al., 2021; Herpich et al., 2019). The consistent modulatory e ects of high-frequency tRNS on VPL might be a result of strengthened attentional network. Functional connectivity within the attentional network was found to be increased after high-frequency tRNS, which was positively correlated with the magnitude of improvement in task performance (Conto et al., 2021).

We found that occipital 10-Hz tACS boosted VPL e ciently. Notably, more subjects were added in the present study, making our previous ndings more robust (He, Yang, & Gong, 2022). In our previous study, we found that tACS boosts orientation discrimination learning in a frequency- and location-speci c manner. Speci cally, occipital 10-Hz tACS administrated during training resulted in the subjects learning to discriminate the orientations of task stimuli faster and achieving greater improvement compared with the sham 10-Hz stimulation condition. Furthermore, the modulatory e ect was absent in other stimulation conditions, such as occipital tACS at other alternating frequencies (6, 20, and 40 Hz) and 10-Hz tACS over other cortical regions (He, Yang, & Gong, 2022). Additionally, in another study, researchers found that tACS at 3 Hz was not e ective in modulating VPL (Zizlsperger et al., 2016). Taken together, these results demonstrate that occipital tACS modulates VPL in a frequency-speci c manner, providing strong evidence for the vital role of alpha oscillations in gating VPL (Bays, Visscher, Le Dantec, & Seitz, 2015; Michael, Covarrubias, Leong, & Kourtzi, 2023).

Further, we also found that occipital 10-Hz tACS showed a stronger modulatory e ect than occipital tRNS in visual perceptual learning. It should be pointed out that this study is the rst investigation, to the best of our knowledge, to compare the modulatory e ects of tACS and tRNS on VPL. Di erences found in the modulatory e ects on VPL between 10-Hz tACS and tRNS might re ect the inherent dissimilarities between these two types of tES techniques in modulating attention-related cognitive processing. It has been clearly demonstrated that 10-Hz tACS can directly entrain alpha power by aligned phase coherence or spike-timing (Huang et al., 2021; Johnson et al., 2020; Krause et al., 2019), such that attention-related cognitive processing is strengthened by occipital tACS at 10 Hz directly (Clayton, Yeung, & Cohen Kadosh, 2019). In contrast, high-frequency tRNS over the occipital regions may not modulate attentional processing e ciently. Previous studies have shown that applying high-frequency tRNS over the parietal regions can improve visual attention (Edwards, Contò, Bucci, & Battelli, 2020; Shalev, De Wandel, Dockree, Demeyere, & Chechlacz, 2018; Tyler, Conto, & Battelli, 2018), but no such e ect was observed when stimulating the visual areas (Conto et al., 2021; Conto, Tyler, Paletta, & Battelli, 2023; Tyler et al., 2018). Therefore, the superior modulatory e ects of occipital 10-Hz tACS on VPL compared to high-frequency tRNS may be attributed to di erent e cacies to mediate attentional processes. Here, this explanation is referred to as the e cacy of attention hypothesis, which requires further investigation in the future.

Our ndings will provide a practical guide for vision rehabilitation. VPL has been widely adopted to restore low-vision in neuroophthalmology (Lu et al., 2016). In practice, it is a common desire of patients and their families to achieve the best e ect in a short course of treatment (He, Yang, & Gong, 2022). However, typical clinic-oriented studies require weeks to months of training and consist of thousands of trials, placing a signi cant economic and psychological burden on both the patients' families and society in general (Herpich et al., 2019). Therefore, developing methods that can speed up the process and improve the treatment e ectiveness is currently a hot research topic. Our results show that 10-Hz tACS over visual areas during training accelerated the learning process and maximized learning gains in healthy adults, ndings that are expected to be signi cant for patients who need to learn or relearn skills due to injuries or illnesses. Overall, our

ndings have the potential to signi cantly impact the eld of vision habilitation (Herpich et al., 2019; Huang et al., 2022; Wu et al., 2023), and further studies will help to fully determine the e ectiveness of this method for patients. For example, researchers have found that patients with cortical blindness (vision loss caused by damage to the primary visual cortex) regained the ability to discriminate visual motion direction after extensive training concurrent with high-frequency tRNS (Herpich et al., 2019). The current study, however, has potential limitations with regard to clinical applications. For example, in this study, the majority of the participants were under the age of 30 years, and it is unclear if the protocols employed would be applicable to other populations (e.g., those of an elderly age) or other training tasks.

Keywords: transcranial electrical stimulation, tDCS, tACS, tRNS, visual perceptual learning, visual plasticity, unsupervised learning, implicit learning

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